Development of Discriminating Method for Dissolution of Aceclofenac Marketed Formulations

Tejal Soni1,4, Chirag Nagda2, Tejal Gandhi2, and N. P. Chotai3
1 Department of Pharmaceutics, Anand Pharmacy College, Anand, Gujarat, India
2 Department of Pharmaceutics, Indukaka College of Pharmacy, New Vallabh-Vidyanagar, Gujarat, India
3 Department of Pharmaceutics, A. R. College of Pharmacy, Vallabh-Vidyanagar, Gujarat, India

ABSTRACT
The development of a meaningful dissolution procedure for drug products with limited water solubility has been a challenge to the pharmaceutical industry. Aceclofenac (BCS Class II drug) is a nonsteroidal anti-inflammatory drug. There is no official dissolution medium available in the literature. In the present study, parameters such as solubility, medium pH, surfactant type, dissolution behavior of formulations, influence of sink conditions, stability, and discriminatory effect of dissolution testing were studied for the selection of a proper dissolution medium. Results of solubility data revealed that solubility increased with an increase in pH. Sink conditions were exhibited in all media except double-distilled water and 0.1 N HCl. The drug and marketed formulations were stable in the dissolution media used. An agitation speed of 50 rpm showed a more discriminating drug release profile than 75 rpm. The discriminating dissolution method for aceclofenac formulation is paddle at 50 rpm, 900 mL pH 6.8 phosphate buffer, greater than 80% of the label amount is released over 60 minutes.

INTRODUCTION
The development of a meaningful dissolution procedure for drug products with limited water solubility has been a challenge to both the pharmaceutical industry and the agencies that regulate them. Low-solubility drugs are usually lipophilic, and drug release is usually the rate-limiting process for oral drug absorption of these substances (1–3). Both in vivo physiology and the physicochemical characteristics of the drugs are important to the oral absorption of poorly water-soluble drugs. In vivo, the dissolution process depends on physicochemical parameters, which may be affected by the intraluminal conditions in the body. Naturally occurring surfactants solubilize sparingly soluble drugs in the body and help in the absorption process. A dissolution medium containing surfactant can better simulate the environment of the gastrointestinal tract than a medium containing organic solvents or other non-physiological substances, making the dissolution test conditions more useful in evaluating drug quality (4, 5). Specific information about the drug substance solubility, drug substance stability as a function of pH, and BCS Classification will direct the expedient selection of a proper dissolution medium. A sensitive, reliable in vitro dissolution procedure is used to determine the quality of a product and to advance the evolution of dissolution technology. A clear trend has emerged where the dissolution test has moved from a traditional quality control test to a surrogate in vitro bioequivalence (BE) study (6, 7).

Aceclofenac (BCS Class II drug) is a non-steroidal anti-inflammatory drug that acts via multifactor mechanisms and is used to treat pain and inflammation. It is practically insoluble in water. Because there is no official dissolution medium available in the monographs, the objective of this study was to develop a discriminating dissolution method for aceclofenac solid oral dosage forms to support product development and quality control efforts.

EXPERIMENTAL
Materials
Aceclofenac was a gift from Mepro Pharmaceutical Pvt. Ltd, Surendranagar. Sodium lauryl sulfate (SLS), Tween 80, potassium dihydrogen orthophosphate, sodium dihydrogen orthophosphate (Qualigens, Mumbai), sodium hydroxide (S.D. Fine chemicals, Mumbai), methanol (AR grade), and hydrochloric acid (Merck, Darmstadt, Germany) were used. Double-distilled water was used throughout the study.

Methods
Saturation Solubility Study
The saturation solubility of aceclofenac (ACE) was determined in the following: double-distilled water; 0.6, 0.8, 1.0, 1.5, and 2% (w/v) SLS in water; 0.1, 0.2, 0.5, 1, and 2% Tween in water; 0.1 N HCl; pH 4.5 acetate buffer; and pH 6.8 phosphate buffer at 37 °C. Excess ACE was added to
100 mL of dissolution medium in a conical flask and agitated continuously at room temperature for 8 h on a shaker. The solutions were kept aside for 6 h until equilibrium was achieved. The solutions were then filtered through No. 41 Whatman filter paper, and the filtrate was suitably diluted and analyzed spectrophotometrically at 275 nm (UV–vis spectrophotometer, Shimadzu-1750).

**In Vitro Drug Release Study**
A batch of 20 tablets of ACE was procured for comparative studies of different brands. The dissolution experiment was performed using USP Apparatus 2 at 37 ± 2 °C with paddle speeds of 50 ± 5 rpm and 75 ± 5 rpm in 900 mL dissolution medium (Electrolab, TOD-08L). A 5-mL sample was withdrawn at different time intervals and analyzed spectrophotometrically after every 24-h period. Each day the concentrations of drug found in the standard and formulation were compared with concentrations of drug found in the same samples stored at 2–8 °C. The absolute differences between the results at time zero and the time indicated for stability were determined by analyzing the content using a UV–vis spectrophotometer.

**Stability Study**
Solutions of pure ACE and drug formulation A (after dissolution) in different media were stored in the dark at ambient temperature and at 2–8 °C. The concentrations of drug found in the standard and formulation were compared with concentrations of drug found in the same samples stored at 2–8 °C. The absolute differences between the results at time zero and the time indicated for stability were determined by analyzing the content using a UV–vis spectrophotometer.

**Comparison of Dissolution Profiles by a Model-Independent Method**
This study utilized a model-independent approach in which the dissolution profiles of two drug products are compared using the fit factor. This fit factor directly compares the difference between percent drug dissolved per unit time for a test and a reference product. The fit factor, \( f_2 \), is defined by the following:

\[
f_2 = 50 \log \left[ 1 + \left( \frac{1}{n} \sum_{t=1}^{n} \left( \frac{R_t - T_t}{R_t} \right)^2 \right)^{0.5} \times 100 \right]
\]

where \( n \) is the number of dissolution sampling times, and \( R_t \) and \( T_t \) are the individual or mean percent dissolved at each time point for the reference and test dissolution profiles, respectively (17).

**RESULTS**
The results of the solubility study and the influence of sink conditions are summarized in Table 1 and show that there was a significant increase in solubility with increasing pH. The solubility of ACE in double-distilled water was found to be 58.67 µg/mL. The addition of different concentrations of SLS significantly increased solubility by up to 13.4-fold. Solubility decreased with Tween 80 at concentrations of 1% and higher. The maximum solubility was 1538 µg/mL in pH 6.8 phosphate buffer (Figure 1).

<table>
<thead>
<tr>
<th>Dissolution Medium</th>
<th>Solubility (mean ± SD) µg/mL</th>
<th>Sink Condition C/Cd</th>
</tr>
</thead>
<tbody>
<tr>
<td>Double-distilled water</td>
<td>58.67 ± 0.101</td>
<td>0.52803</td>
</tr>
<tr>
<td>0.6% w/v SLS in D.D. water</td>
<td>453.2 ± 1.295</td>
<td>4.0788</td>
</tr>
<tr>
<td>0.8% w/v SLS in D.D. water</td>
<td>466.6 ± 2.185</td>
<td>4.1994</td>
</tr>
<tr>
<td>1% w/v SLS in D.D. water</td>
<td>731.7 ± 0.952</td>
<td>6.583</td>
</tr>
<tr>
<td>1.5% w/v SLS in D.D. water</td>
<td>724.69 ± 0.877</td>
<td>6.522</td>
</tr>
<tr>
<td>2% w/v SLS in D.D. water</td>
<td>813.36 ± 1.144</td>
<td>7.3202</td>
</tr>
<tr>
<td>0.2% w/v Tween 80 in D.D. water</td>
<td>855.17 ± 2.44</td>
<td>7.6965</td>
</tr>
<tr>
<td>0.5% w/v Tween 80 in D.D. water</td>
<td>1019.8 ± 1.187</td>
<td>9.178</td>
</tr>
<tr>
<td>1% w/v Tween 80 in D.D. water</td>
<td>798.8 ± 1.153</td>
<td>7.1892</td>
</tr>
<tr>
<td>2% w/v Tween 80 in D.D. water</td>
<td>782.0 ± 1.89</td>
<td>7.038</td>
</tr>
<tr>
<td>0.1 N HCl (pH 1.2)</td>
<td>21.93 ± 0.257</td>
<td>0.1973</td>
</tr>
<tr>
<td>Acetate buffer pH 4.5</td>
<td>995.0 ± 0.810</td>
<td>8.955</td>
</tr>
<tr>
<td>Phosphate buffer pH 6.8</td>
<td>1538.7 ± 1.215</td>
<td>13.84</td>
</tr>
</tbody>
</table>

*\( C_d \) indicates saturation solubility of aceclofenac in 900 mL dissolution medium; \( C_r \) dose of aceclofenac in tablet formulation; D.D indicates double-distilled; and SLS is sodium lauryl sulfate.

Figure 1. pH–solubility profile of aceclofenac. Each point refers to mean ± SD (n=3).
addition of surfactant at concentrations of 1% and higher (Figure 2). Greater than 80% drug release was found within 60 min in pH 6.8 phosphate buffer medium.

Table 2 contains a summary of the stability data for standards and samples. The absolute difference between the concentrations of drug stored at 2–8 °C and the same solution at room temperature over the period of 7 days was found to be less than 3.0% for all media. Correlation of the solubility data, stability data, and influence of sink conditions showed pH 6.8 phosphate buffer to be a suitable medium.

The percentage cumulative drug release (% CDR) for marketed formulations A, B, and C in pH 6.8 phosphate buffer was compared at 50 ± 5 rpm and 75 ± 5 rpm (Figures 3 and 4). Table 3 contains the statistical evaluation of the cumulative drug release percentage at 50 and 75 rpm for film-coated tablets A, B, and C using the Student’s t-test at the 5% significance level. The P value less than or equal to the delineated significance level (0.05) indicates that there is a statistically significant difference in the drug release in formulations at varying speeds of rotation. A significant difference in % CDR was found for formulations A and C with varying speed, while no statistically significant difference was found for formulation B (ACE with β-cyclodextrin).

Table 4 shows a comparison of the dissolution profiles of marketed products using the similarity factor f² at different stirring speeds in pH 6.8 phosphate buffer. Similarity was found in formulations B and C with reference product A at 75 ± 5 rpm, while dissimilarity was found in formulation B with reference product A at 50 ± 5 rpm.
Dissolution expressed as attributed to the micellar solubilization by SLS. This significant increase is with an increase in buffer pH as well as with an increase in saturation solubility of ACE in different media increased correctly, can approximate the GI fluid condition. If surfactant is a reasonable approach, which if implemented that solubility increases with pH. However, the addition of insoluble in water. ACE is a weak acid, and it is expected solubility. ACE is a lipophilic compound and is practically modifications in the dissolution medium to increase the solubility. ACE is a lipophilic compound and is practically insoluble in water. ACE is a weak acid, and it is expected that solubility increases with pH. However, the addition of surfactant is a reasonable approach, which if implemented correctly, can approximate the GI fluid condition.

Saturation solubility of ACE in different media increased with an increase in buffer pH as well as with an increase in surfactant concentration. This significant increase is attributed to the micellar solubilization by SLS.

The ratio of solubility to drug concentration (dose), expressed as \( C_s / C_d \) represents the closeness to sink conditions; a sink condition occurs when the amount of drug that can be dissolved in the dissolution medium is three times greater than the amount of drug to be dissolved. A low \( C_s / C_d \) ratio shows the existence of non-sink conditions. The rate of drug dissolution will be slowed by the limited solubility of the drug in that medium.

In the case of a higher percentage of Tween 80 as compared with SLS, drug dissolution rate was reduced. The reason for this may be that drug dissolution is the result of drug liberation and drug diffusion into the dissolution medium. In this respect, the diffusivity of dissolved species (drug molecule and drug–micelle complex) plays an important role. The diffusivity of drug–micelle complex is several-fold less than for drug alone, and the net change in the dissolution rate is the sum of solubility enhancement and a decline in effective diffusivity. The higher molecular weight of Tween 80 (1310 versus 288.4 g/mol) and the greater aggregation weight of its micelles (76,000 versus 15,900 g/mol) compared with SLS result in lower diffusivity of drug-micelle complex and hence a reduction in the dissolution rate (8–9).

A dissolution medium need not be chosen if the standard solutions are not stable for at least 24 h at ambient temperature (10). In the present study, the drug was found to be stable in various media alone and in the presence of excipients.

The discriminating power of the method was evaluated by testing three marketed formulations (A, B, and C) having different compositions, of which formulation B contained ACE with \( \beta \)-cyclodextrin. The most common way to challenge the discriminatory power of the method is to test formulations with differences resulting from changes in the characteristics of the API, drug product composition, product manufacturing process, and stability conditions (11–16). In general, mild agitation conditions should be maintained during dissolution testing to allow maximum discriminatory power (4). In most cases, the dissolution apparatus tends to become less discriminating when operated at faster speeds that result in a flatter drug release profile. For the present study, it can be concluded that the drug release profile at 50 ± 5 rpm detected small changes in a drug product composition. At 75 ± 5 rpm, dissolution proceeded too quickly and produced a profile that leveled off too early to show discrimination between the formulations. The satisfactory discriminatory power was observed in dissolution at 50 rpm.

The FDA guidances on dissolution testing of immediate-release solid oral dosage formulations (15) and bioavailability and bioequivalence studies for oral dosage forms (16) recommend the use of a model-independent mathematical approach proposed by Moore and Flanner (17–22) for calculating similarity factor. An \( f_2 \) value between 50 and 100 represents similarity. In the present study, at the speed of 75 rpm, similarity was found in formulations B and C, while at 50 rpm, similarity was not found in formulation B. It can be concluded that the drug release profile at 50 rpm detected small changes in drug product composition. The satisfactory discriminatory power was observed in dissolution at 50 rpm.

**DISCUSSION**

A dissolution study of dosage forms necessitates modifications in the dissolution medium to increase the solubility. ACE is a lipophilic compound and is practically insoluble in water. ACE is a weak acid, and it is expected that solubility increases with pH. However, the addition of surfactant is a reasonable approach, which if implemented correctly, can approximate the GI fluid condition.

Table 3. Statistical Evaluation of Dissolution Results for Formulation A, B, and C Film-Coated Tablets at Different Stirring Speeds in pH 6.8 Phosphate Buffer Medium.

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Time</th>
<th>50 rpm</th>
<th>75 rpm</th>
<th>t-test</th>
<th>P value</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>0</td>
<td>0</td>
<td>0</td>
<td></td>
<td></td>
</tr>
<tr>
<td>A</td>
<td>15</td>
<td>49.95</td>
<td>90.29</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>30</td>
<td>74.496</td>
<td>99.34</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>45</td>
<td>77.622</td>
<td>100.2</td>
<td>2.38</td>
<td>0.05</td>
</tr>
<tr>
<td></td>
<td>60</td>
<td>100.024</td>
<td>100.98</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>75</td>
<td>100.49</td>
<td>103.9</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>90</td>
<td>100.5</td>
<td>105.89</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Table 4. Comparison of Film-Coated Tablet Dissolution Profiles through the Similarity Factor (\( f_2 \)) at Different Stirring Speeds in pH 6.8 Phosphate Buffer.

<table>
<thead>
<tr>
<th>Stirring Speed (rpm)</th>
<th>Formulation B</th>
<th>Formulation C</th>
</tr>
</thead>
<tbody>
<tr>
<td>50</td>
<td>44.11</td>
<td>67.62</td>
</tr>
<tr>
<td>75</td>
<td>68.075</td>
<td>73.266</td>
</tr>
</tbody>
</table>

Formulation A is reference product.
CONCLUSION
Dissolution testing is a very important in vitro test for evaluating drug products. Because there is no dissolution method specified for aceclofenac in the literature, an attempt was made to develop a dissolution method that is discriminating. The use of 900 mL of pH 6.8 phosphate buffer at 37 ± 2 °C, a paddle speed of 50 ± 5 rpm for film-coated formulations, and a 60-min test provided satisfactory results for all products.

ACKNOWLEDGMENT
The authors are thankful to Mepro Pharmaceutical Pvt. Ltd, Surendranagar, for providing aceclofenac as a gift sample.

References
18. Podczeck, F. Comparison of in vitro dissolution profiles by calculating mean dissolution time (MDT) or mean residence time (MRT). Int. J. Pharm. 1993, 97, 93–100.